

DEVELOPMENT OF GRIPPING ASSISTIVE DEVICE  
FOR TRAINING

BY

MOHD RAIS HAKIM BIN RAMLEE

A dissertation submitted in fulfilment of the requirement for  
the degree of Master of Science (Mechatronics Engineering)

Kulliyyah of Engineering  
International Islamic University Malaysia

SEPTEMBER 2020

## ABSTRACT

Gripping is an everyday task which goes unnoticeable. Since it is an essential daily movement, without this motion, a lot of activities involving this movement could not be done. However, due to the growing process or some injury, the grasping movement become disrupted, which cause difficulties to do some daily activities. These impacts depend on individual and also in different ways regardless of age and how the body drastically become weak and fragile, less adaptable and less impervious to sickness and damage. Patients affected with hand gripping issues typically require long term care. This also contributes towards their ability to recover much longer as their regular activity reduces and dependency on other increases. Therapy, as an early rehabilitation within the golden period (less than 3 three months prior to incident), is required to improve the gripping motion and regain back the strength of the affected joints as well as muscles. Rehabilitation also helps to improve the patient's ability to return the patient to the level of premorbid function. The current situation is that the rehabilitation process takes longer as there are few physiotherapists available in hospitals. It is anticipated that a mechatronics approach using robotics-based devices have been seen as a promising candidate to assist existing forms of the rehabilitation process. The idea is to develop a basic function rehabilitation robot to support the physiotherapist. The rehabilitation robot is designed to help with the gripping process, where the system is based on a master-slave mechanism which needs a healthy hand to control the weak hand. The system uses a leap motion sensor as an input, and the output is an exoskeleton. A gyroscope was used to indicate the finger position and placed on top of the exoskeleton. The exoskeleton has been tested by a subject for several times. The results shows the simulation of exoskeleton that can do flexion and extension process. The errors between the desired extension angle value and the extension angles on link 1 and link 2 are 5.58% and 11.02% respectively. However, this design need some improvement on the material and angle sensors selection. The material must be light and smooth surface and the angle sensor must be high in precision and accuracy.

## خلاصة البحث

إن إمساك أي شيء مهمة يومية التي غير ملحوظة. ولا يمكن القيام بالكثير من الأنشطة التي تنطوي عنها بدون هذه الحركة لأنها حركة يومية أساسية. ولكن بسبب العمليات المتنامية أو بعض الإصابات، قد تعطل حركة إمساك الشيء مما يسبب صعوبات في القيام ببعض الأنشطة اليومية. وتعتمد هذه التأثيرات على الأفراد والأساليب بغض النظر على العمر وكذلك ضعف حركة الجسم، أقل تكيفاً وقدرة في حالة المرض والأضرار. كهذا، إن المرضى الذين يعانون من مشاكل في الإمساك باليد يحتاجون إلى العلاج لمدة طويلة. وهذا يساهم في تعزيز قدرتهم على التعافي لأطول فترة مع الانخفاض نشاطهم المنتظم وزيادة الاعتماد على الآخرين. والعلاج هو إعادة التأهيل في فترة مبكرة (أقل من ثلاثة أشهر من وقوع الحادث)، وال المطلوب على التحسين حركة الإمساك واستعداد إلى قوة المفصل المتضررة وكذلك بالعضلات. إن التأهيل يساعد على تحسين قدرة المريض وإعادته إلى المستوى السابق. والحالة الراهنة هي أن عملية إعادة التأهيل تستغرق وقتاً أطول لأن هناك قليل من الفيزيائيين المتاحين في المستشفيات. ومن المتوقع أن الميكاترونكس باستخدام الأجهزة التي تستند إلى الإنسان الألى اعتبر مرشحة لعدة لمساعدة الأشكال القائمة لعملية إعادة التأهيل. وتتلخص الفكرة في تطوير روبوت أساسي للوظائف إعادة تأهيل دعماً للمعالجين الفيزيائيين. لقد تم تصميم روبوت لإعادة التأهيل ومساعدة عملية الإمساك، حيث يستند النظام على الآلية الرئيسية التي تحتاج إلى اليد الصريحة للسيطرة على اليد المتضررة. ويستخدم النظام المستشعر الحركة كإدخال، والهيكل الخارجي كالإنتاج. وتم استخدام الجيروسكوب للإشارة إلى موضع الإصبع و موضع فوق الهيكل الخارجي. وقد تم اختبار الهيكل من قبل المشاركين لعدة مرات. لوضع النتائج محاكاة الهيكل الخارجي الذي يمكن أن يقوم به المرونة وعملية التمديد. الأخطاء بين قيمة الزاوية الامتداد المطلوبة وزاوية الامتداد في لارتباط 1 والارتباط 2 ونسبتهما 5.58% و 11.02% على التوالي. ومع ذلك، يحتاج هذا التصميم إلى بعض التحسينات في تحديد المواد ومستشعرات الزوايا. يجب أن تكون المادة سطحاً خفيفاً وناعماً. ويجب أن يكون مستشعر الزاوية عالي الدقة والدقة.

## APPROVAL PAGE

I certify that I have supervised and read this study and that in my opinion, it conforms to acceptable standards of scholarly presentation and is fully adequate, in scope and quality, as a dissertation for the degree of Master of Science (Mechatronics Engineering).

.....  
Hazlina MD. Yusof  
Supervisor

.....  
Shahrul Na'im Sidek  
Co-Supervisor

I certify that I have read this study and that in my opinion it conforms to acceptable standards of scholarly presentation and is fully adequate, in scope and quality, as a dissertation for the degree of Master of Science (Mechatronics Engineering).

.....  
Ahmad Jazlan bin Haja Mohideen  
Internal Examiner

.....  
Azhar bin Mohd Ibrahim  
Internal Examiner

This dissertation was submitted to the Department of Mechatronics Engineering and is accepted as a fulfilment of the requirement for the degree of Master of Science (Mechatronics Engineering).

.....  
Syamsul Bahrin Abdul Hamid  
Head, Department of  
Mechatronics Engineering

This dissertation was submitted to the Kulliyah of Engineering and is accepted as a fulfilment of the requirement for the degree of Master of Science (Mechatronics Engineering).

.....  
Sany Izan Ihsan  
Dean, Kulliyah of Engineering

## DECLARATION

I hereby declare that this dissertation is the result of my own investigations, except where otherwise stated. I also declare that it has not been previously or concurrently submitted as a whole for any other degrees at IIUM or other institutions.

Mohd Rais Hakim Bin Ramlee

Signature .....

Date .....

**INTERNATIONAL ISLAMIC UNIVERSITY MALAYSIA**

**DECLARATION OF COPYRIGHT AND AFFIRMATION OF  
FAIR USE OF UNPUBLISHED RESEARCH**

**DEVELOPMENT OF GRIPPING ASSISTIVE DEVICE FOR  
TRAINING**

I declare that the copyright holders of this dissertation are jointly owned by the student and IIUM.

Copyright © 2020 Mohd Rais Hakim Bin Ramlee and International Islamic University Malaysia. All rights reserved.

No part of this unpublished research may be reproduced, stored in a retrieval system, or transmitted, in any form or by any means, electronic, mechanical, photocopying, recording or otherwise without prior written permission of the copyright holder except as provided below

1. Any material contained in or derived from this unpublished research may be used by others in their writing with due acknowledgement.
2. IIUM or its library will have the right to make and transmit copies (print or electronic) for institutional and academic purposes.
3. The IIUM library will have the right to make, store in a retrieved system and supply copies of this unpublished research if requested by other universities and research libraries.

By signing this form, I acknowledged that I have read and understand the IIUM Intellectual Property Right and Commercialization policy.

Affirmed by Mohd Rais Hakim Bin Ramlee

.....  
Signature

.....  
Date

## **ACKNOWLEDGEMENTS**

Firstly, I am thankful to Allah SWT for all His blessings because He is the One who help me to finish my research paper. A special thanks to Dr. Hazlina Md Yusof and Dr. Shahrul Na'im Sidek, my supervisors who has guided me through this semester. They encourage me and helped me to understand more about the research. Dr. Hazlina Md Yusof is a very kind person. She sacrifices most of her time to give advices on doing the research properly. I also would like to thank to my friends, Ismail and Ikmal, who have been helping me in many ways. They are very kind and supported me a lot during doing the project. Last but not least, I would like to thank to my family and others who have involved in my project directly or indirectly.

# TABLE OF CONTENTS

Abstract .....	II
Abstract in Arabic.....	III
Approval Page .....	IV
Declaration .....	V
Copyright Page.....	VI
Acknowledgements .....	VII
List of Figures .....	X
List of Tables.....	XII
List Of Symbols.....	XIII
List Of Abbreviation.....	XIV
<b>CHAPTER ONE: INTRODUCTION.....</b>	<b>1</b>
1.1 Introduction.....	1
1.2 Problem Statement .....	3
1.3 Research Objective.....	4
1.4 Scope of Research .....	4
1.6 Thesis Organization.....	6
<b>CHAPTER TWO: LITERATURE REVIEW .....</b>	<b>8</b>
2.1 Hand Anatomy .....	8
2.2 Hand Forces And Torque.....	9
2.3 Grip.....	11
2.4 Hand Rehabilitation.....	13
2.5 Self-Motion Control System .....	14
2.6 Hand Motion Rehabilitation Devices .....	15
2.6.1 Actuator System .....	16
2.6.2 Kinect Motion Sensing device .....	17
2.6.3 Leap Motion Sensor .....	18
2.6.4 MPU 9250: Three-axis gyroscope , triaxial accelerometer and triaxial magnetic field.....	19
2.6.5 Complementary filter.....	19
2.7 Summary.....	20
<b>CHAPTER THREE: RESEARCH METHODOLOGY .....</b>	<b>22</b>
3.1 Introduction.....	22
3.2 Research Design.....	22
3.3 Component Selection.....	23
3.3.1 Leap Motion Sensor .....	23
3.3.2 Microcontroller .....	24
3.3.3 Servomotor.....	25
3.3.4 MPU-9250: Three-axis Gyroscope, Tri-axial Accelerometer and Tri- axial Magnetic field.....	26
3.3.5 PLA Plastic .....	27
3.4 Mechanical Design .....	27
3.4.1 Mechanical construction.....	28



3.4.2	Actuator part .....	29
3.4.3	Sensor Equipment.....	30
3.5	Circuit Diagram.....	31
3.6	Workflow Design .....	32
3.7	Microcontroller Program .....	33
3.8	Data Collection.....	35
3.9	Summary .....	35
<b>CHAPTER FOUR: RESULT AND DISCUSSION .....</b>		<b>36</b>
4.1	Introduction.....	36
4.2	Simulation on Solidwork .....	36
4.3	Experimental Setup .....	38
4.4	Results.....	42
4.5	Strain, Stress and Fatigue Analysis .....	46
4.6	Summary .....	51
<b>CHAPTER FIVE: CONCLUSION AND RECOMMENDATION .....</b>		<b>52</b>
5.1	Conclusion .....	52
5.2	Limitation.....	53
5.3	Recommendation and Future Works .....	54
<b>REFERENCES .....</b>		<b>55</b>
<b>APPENDIX A: COMPONENT LIST AND SOFTWARE.....</b>		<b>57</b>
<b>APPENDIX B: PROGRAMMING CODE .....</b>		<b>58</b>

## LIST OF FIGURES

Figure 1.1 Flowchart of Research Methodology	6
Figure 2.1 Joints in human skeletal system	9
Figure 2.2 Natural Hand's Contact Forces	10
Figure 2.3 The force during holding an object at different torque	11
Figure 2.4 Eight Hand Therapy Ball Exercises	11
Figure 2.5 Self – Motion Control	15
Figure 2.6 HWARD (Hand Wrist Assisting Robotic Device)	17
Figure 2.7 Construction of the Leap Motion Controller	18
Figure 2.8 MPU9250	19
Figure 3.1 Flowchart of research design process	23
Figure 3.2 Leap motion sensor	23
Figure 3.3 Arduino UNO	24
Figure 3.4 Digital Servomotor	25
Figure 3.5 MPU9250	26
Figure 3.6 Top View of Exoskeleton.	28
Figure 3.7 Side View of Exoskeleton	29
Figure 3.8 Connection between motors and links	30
Figure 3.9 Connection between sensors and links	30
Figure 3.10 Schematic Diagram of Arduino connected to the Servomotors	31
Figure 3.11 Schematic Diagram of Arduino connected to the Angle Sensors	32
Figure 3.12 Block Diagram of Workflow Design	33
Figure 3.13 Flowchart of the first microcontroller system	34
Figure 4.1 Maximum Extension	37

Figure 4.2 Maximum Flexion	37
Figure 4.3 Visual Output of Simulation Results	38
Figure 4.4 Visual Positioning of User	39
Figure 4.5 Setting up Leap Motion Sensor and Exoskeleton	39
Figure 4.6 Calibration of Leap Motion	40
Figure 4.7 Calibrating with Leap Motion Sensor.	40
Figure 4.8 (a)Top View of Flexion Position (b)Whole View of Flexion Process	41
Figure 4.9 (a)Top View of Extension Position (b)Whole View of Extension Process	41
Figure 4.10 Angular Position of Link 1	43
Figure 4.11 Angular Position for Link 2	44
Figure 4.12 Variation of Angular Position of Link 1 and Link 2	45
Figure 4.13 Static Structural	46
Figure 4.14 Total Deformation	47
Figure 4.15 Equivalent Stress	47
Figure 4.16 Equivalent Elastic Strain	48
Figure 4.17 Fatigue Life	49
Figure 4.18 Fatigue Damage	49
Figure 4.19 Safety Factor	50
Figure 4.20 Fatigue Sensitivity	51

## LIST OF TABLES

Table 2.1 Summary of Strategy Used	20
Table 4.1 Flexion and Extension Angle of Link 1	43
Table 4.2 Flexion and Extension Angle of Link 2	44
Table 4.3 Average of Flexion and Extension Angle of Link 1 and Link 2	45

## LIST OF SYMBOLS

V	Voltage
v	Speed
$\mathcal{T}$	Torque
$\rho$	Density
E	Young's Modulus
$\theta$	Degree
F	Force
$\sigma$	Stress
$\varepsilon$	Elastic Strain
$\tau$	Shear Stress
SF	Safety Factor

## LIST OF ABBREVIATIONS

MMA	Malaysian Medical Association
CAM	Complementary and Alternative Medicine
NCCAM	National Centre for Complementary and Alternative Medicine
HOWARD	Hand-Wrist Assisting Robotic Device
PP	Proximal Phalange
MP	Middle Phalange
DP	Distal Phalange
MCP	Metacarpo Phalange
PIP	Proximal Interphalange
DIP	Distal Interphalange
EMG	Electromyography
API	Application Programming Interface
USB	Universal Serial Bus
LED	Light Emitting Diode
IR	Infrared
IMU	Inertial Measurement Unit
PWM	Pulse Width Modulation
ADC	Analog Digital Converter
PLA	Polyactide
DOF	Degree of Freedom

COM      Communication

# **CHAPTER ONE**

## **INTRODUCTION**

### **1.1 INTRODUCTION**

Those aged 60 years and above are defined as elderly, as recommended by the Malaysian Medical Association (MMA). According to the Department of Statistics Malaysia (Census 2000), the Malaysian elderly population of 60 and above is increasing progressively and is predicted to increase to 3.2 million people by the year 2020. Although this indicates an increase in life expectancy, from healthcare perspective, this reflects that the population will be susceptible to different diseases and morbidities and, therefore, poses a higher demand for all medical and healthcare services. To be precise, Complementary and Alternative Medicine (CAM) found to be used often by the elderly, other than other ages, to improve their health (Mitha et al., 2013).

According to National Centre for Complementary and Alternative Medicine (NCCAM), complementary and alternative medicine (CAM) is defined as a group of diverse medical and healthcare systems, practices, and products that are not generally considered part of conventional medicine. In Malaysia, CAM includes practices such as traditional Malay medicine, Islamic medical practice, traditional Chinese medicine, traditional Indian medicine, homeopathy, and complementary therapies, and excludes medical or dental practices utilized by registered medical or dental practitioners. In one Malaysian study it was reported that 69.4% of the Malaysian population used traditional and complementary medicines in their whole lifetime. The ageing process is natural and affects everyone in different ways. The body naturally becomes weaker, less flexible and less resistant to illness and injury. There are a large number of



disabilities that are common in the elderly such as Parkinson's disease and reduced mobility. Physiotherapy is very important in treating these disabilities by reducing symptoms, adapting function and maintaining quality of life. The health care system in Malaysia is primarily geared towards short term care and hospitalisation. The elderly with their chronic diseases and problems require long term care. Rehabilitation from acute illness often lacks in our hospitals in order to help return the elderly patient to the level of premorbid function.

Rehabilitation is a process by which patients undergo treatment to help them return to healthy life by regaining and relearning the skills of everyday living (Maciejasz, Eschweiler, Gerlach-Hahn, Jansen-Troy, & Leonhardt, 2014). Elderly rehabilitation is maintaining and improving the general health and ability of elderly individuals. It also focuses on facilitating the patient to understand and comply challenges, prevent subsequent problems and instruct family members to participate in a supporting part.

The practice of robotic mechanisms for rehabilitation training is a comparatively recent area within the field of robotics in healthcare and emerged from the concept of adopting robots to assist people with impairments. In return, this has led to the development of various rehabilitation robotic devices. Considering the robot as a new development exercise-tool under the therapist's guidance, the key challenge in the area of rehabilitation robotics is how most the therapist's techniques can be augmented with the advancing robot technology. The robotic devices are able of not only providing more persistent and more approachable therapies but still offering other observations into treatment effectiveness based on their knowledge to measure interaction specifications.

Rehabilitation robots operate close to the human user and should be able to deal with various human joints individually and concurrently to imitate human duties. This calls for a robot design that is reliable and user-friendly. Interaction forces between the human user and the robot should also be taken into consideration in controlling the robot in addition to position. Restoring the muscle to perform a specific task perfectly such as standing, walking, eating and gripping is categorized as rehabilitation. Repetitive process during rehabilitation help to reduce the muscle stiffness. The use of mechanical devices are developed to reduce rehabilitation time process, and waiting time as the therapist is not required to be at the site.

## **1.2 PROBLEM STATEMENT**

As time goes by, due to the new era of globalization and improvement of lifestyle, the number of the physiotherapists needed increases as the numbers of post stroke and old patients are increasing. To overcome this problem, engineers have stepped in developing mechanical devices. Due to the increasing needs of the devices, rehabilitation devices were created such as Hand-Wrist Assisting Robotic Device (HOWARD), Biomove Home Device and Hand of Hope. Many portable devices are needed as it allow patients to do their rehabilitation process on their own and for some cases, in their own place. A lot of mechanical devices have been used in Rehabilitation Centre to help physiotherapists assist elderly to do the rehabilitation process. Furthermore, there are many research has been done regarding the design and development of assistive device for post stroke patients but there are several issues with the design. Based on researches that has been reviewed, among the problems captured are

- 1 Most existing designs of exoskeletons are intricate thus limits the subject movement
2. Therapist observation is still highly required as the current exoskeleton design does not have way to measure the progress of gripping process from the patient.

### **1.3 RESEARCH OBJECTIVE**

The main objective of the research is to develop a prototype of four-fingered hand exoskeleton as a training device to restore the gesture of the hand due to old age with grasping and opening disabilities in their everyday lives. In order to fulfil the research requirement, the research objectives are highlighted as below.

1. To develop a user friendly wearable hand assistive device that can be used for independent therapy.
2. To analyse the performance gripping activities of the use of gripping assistive device.

### **1.4 SCOPE OF RESEARCH**

The scopes of the research are as follows:

- To design an exoskeleton using Solidwork software simulation.
- To ensure the exoskeleton can do extension and flexion in vertical mode.
- The exoskeleton only use proximal and intermediates phalanges
- To use sensor for the purposed mechanism movement control.

### **1.5 RESEARCH FLOW**

This chapter is focus on the procedure of the research, conceptual design and component selection. Several methods have been taken into consideration based on Chapter 2 Literature Review. The work in this chapter focuses on building, development and prototyping the gripping assistive device. To achieve the objective of this research, there are many phases need to be adopted.

The first phase focuses on literature survey on the technical and scientific papers. Investigation on suitable literature is done to obtain technical and scientific information and relevant for the systems based on the objectives. This research will be focuses on the hand and rehabilitation control system.

The next phase is about the design of the exoskeleton. In this research, the exoskeleton is designed using Solidwork. The basic design was adopted based on the designs obtained from the literature review. The third phase is a development of the exoskeleton. The exoskeleton is developed based on the design from the Solidwork software. The development is focusing on the component selection, assembling the parts of exoskeleton and the simulation of the hardware.

The fourth phase is data collection. The data is evaluated by using sensors and make some improvement if necessary. The last phase is a documentation of the research. The flowchart of research methodology will be shown in Figure 1.1.

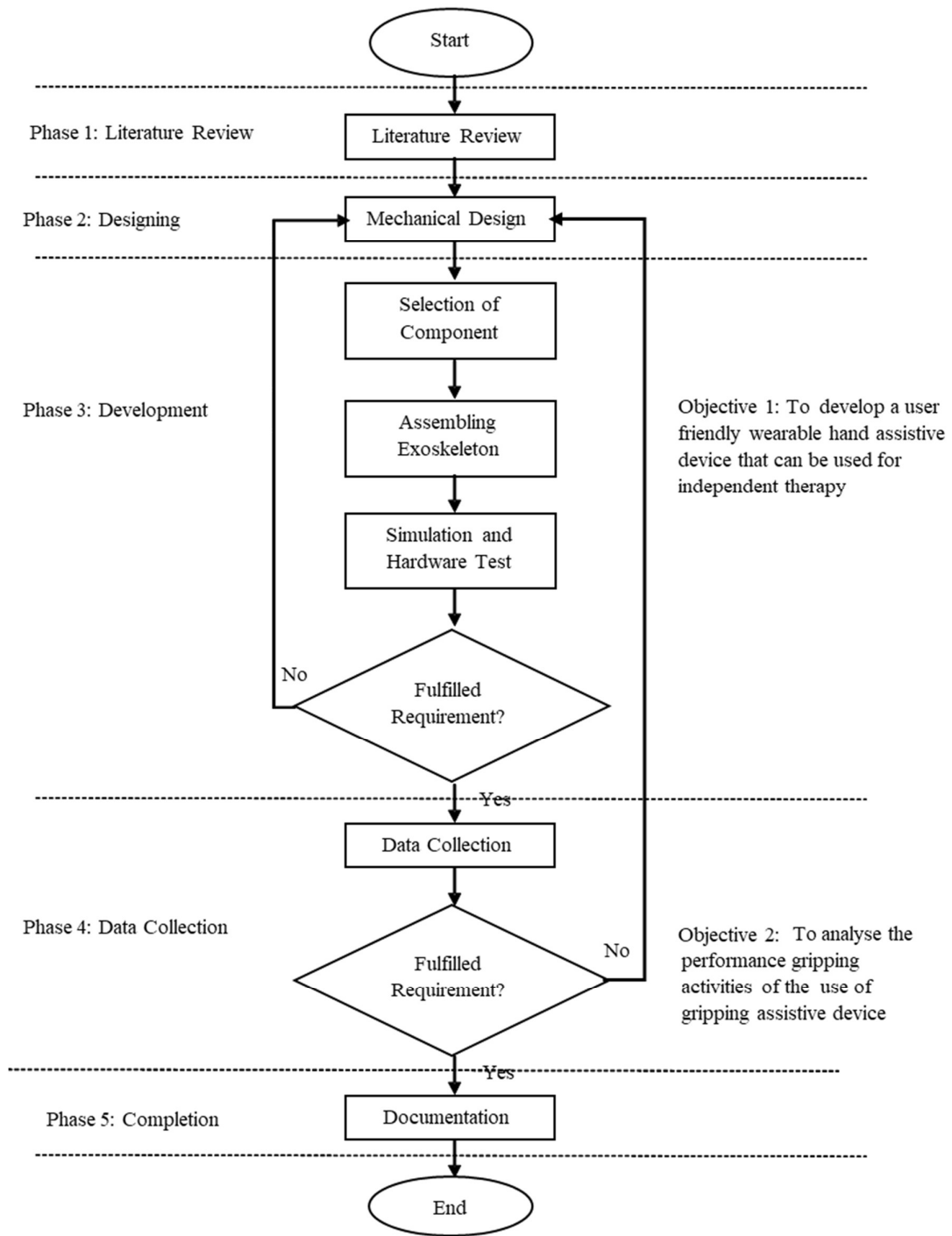


Figure 1.1 Flowchart of Research Methodology

## 1.6 THESIS ORGANIZATION

**Chapter 1:** This chapter discusses about the background of the research and the available rehabilitation process, the purpose of the research. The problem statement is

highlighted in the chapter leads to the objectives of the research. Then the research methodology explains on how the research had been conducted. Finally, the scope of the research is laid out.

**Chapter 2:** This chapter discusses about literature review. Research papers that discusses the same or similar research area within the finger rehabilitation, robotics hand and wearable robotics devices is reviewed based on their objectives, methodologies, problems faced and the components used.

**Chapter 3:** This chapter explains the design involved on the mechanical and electrical system. The design, components and materials selection are elaborated here. The simulation of extension and flexion of the exoskeleton is shown here and the electrical system is presented the selection of actuators, sensors and type of wires is explained through this chapter.

**Chapter 4:** Chapter 4 emphasizes on the result based on the design from Chapter 3 and the analysis that has been done.

**Chapter 5:** Chapter 5 is about the conclusion and some recommendation for future plan of this research.

## **CHAPTER TWO**

### **LITERATURE REVIEW**

In this chapter, the existing proposed approaches are briefly presented and reported which constitutes for dealing with finger rehabilitation. The existing proposed approaches that are reviewed in this chapter covers investigation, analysis or comparison that is significant of developing an exoskeleton for rehabilitation. Finger based rehabilitation has been done by various researchers where most research was their own methods as the mechanism of rehabilitation process with same objective which is to reduce the involvement of therapist. This chapter will briefly explain the various rehabilitation process, hand anatomy, similarities and differences explored by other researches which leads to this research work.

#### **2.1 HAND ANATOMY**

To design the exoskeleton, human hand anatomy has to be studied extensively (Rahman & Al-Jumaily, 2013). The hand has 27 of total bones where eight of them are carpals bone, five in the metacarpals and fourteen remaining is proximal phalanges (PP), middle phalanges (MP) and distal phalanges (DP) (Shahrol Mohamaddan, 2008) Normal human have 5 digits in each hand which consist of four digits (index finger, middle finger, ring finger and little finger) with three phalanges (PP, MP and DP) and one digits (thumb) with only two phalanges (PP and DP). There are joints to connect different phalanges which are Metacarpophalanges (MCP) joints that connect metacarpals with PP, proximal inter-phalangeal (PIP) joints that connect PP and MP and distal inter-phalangeal (DIP) joints that connect MP and DP. PIP is not present in thumb since thumb does not has MP (Surendra WA, Tjahyono AP, 2012). From

previous studies, it can be concluded that our finger contain 3 joints and 3 links for every part of the fingers and 2 joints and 2 links for thumbs. Based on the structure of the hand, each part of the metacarpals bones contain forces and torque which can produce certain movements.

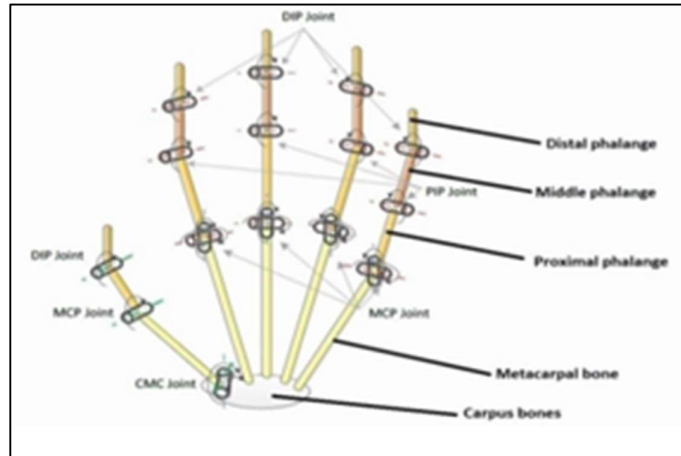


Figure 2.1 Joints in human skeletal system (Surendra WA, Tjahyono AP, 2012)

## 2.2 HAND FORCES AND TORQUE

For the force of the hand, every part of the finger has its own forces. There are lowest contact forces in human hand during gripping (Kargov, Pylatiuk, Martin, Schulz, & Döderlein, 2004). There are 20 positions where the average of the contact force is 0.8N. Additionally, the distal phalanx of the middle and ring finger, and thumb has the highest average forces. The sum of forces is 16.7N while the minimum force at fingertips is 6.3N.